

transferred to subsequent patients or users.

Sterilization methods can be employed on such devices that are reusable in an attempt to disinfect and eliminate microorganisms for subsequent use of the devices. However, some surgical devices contain very small and/or narrow working channels or lumens for performing intricate medical procedures. These small and/or narrow working channels can be difficult to clean and sterilize. If not effectively eliminated, these materials may be transferred to, and potentially cause harmful infections to, other patients or medical personnel through subsequent use of the devices.

In addition to the problems of potential disease transmission and lack of disposability, conventional reusable medical introducer, endoscopes, and the like are subjected to repeated use over prolonged periods. The precision of manipulation and movement in endoscopes and steerable medical devices is often essential for conducting complicated diagnostic and therapeutic medical procedures generally performed with such devices. Some reusable devices containing steering mechanisms often require precision calibration. Further, these devices are regularly subjected to sterilization with heat or chemicals. To accomplish these objectives, conventional reusable devices are often made of stainless steel or other durable materials that are costly. In addition, despite being designed for repeated use, such conventional intricate reusable devices, in particular, such devices that incorporate visualization components, often require regular replacement, further adding to the cost of such devices.

SUMMARY

In some embodiments, the presently disclosed subject matter is directed to an assembly comprising a lumen comprising an open end, a closed end, and a cavity. The assembly further comprises a guiding member comprising a first end, a second end, and a contact element comprising a marker positioned at the second end, wherein the marker is configured to indicate the presence or absence of biological contamination. In some embodiments, the lumen is a working lumen and the cavity is sized and shaped to house a medical device, such as an endoscope. In some embodiments, the guiding member is conically-shaped, with the diameter of the first end less than the diameter of the second end.

In some embodiments, the presently disclosed subject matter is directed to a method of detecting the presence or absence of biological contamination on a medical device. Particularly, the method comprises providing a medical device and providing the disclosed assembly. The medical device is positioned within the cavity of the lumen. At a desired time, the medical device is removed from the cavity of the lumen such that the device contacts the contact element and is exposed to marker. Marker is then detected to determine the presence or absence of biological contamination on the medical device. In some embodiments, the biological contamination comprises bacterial contamination, viral contamination, or combinations thereof. In some embodiments, the detecting comprises exposing the medical device to fluorescence detection, such that if no contamination is present, the marker will not fluoresce and if contamination is present the device will fluoresce.

BRIEF DESCRIPTION OF THE DRAWINGS

Having thus described the disclosure in general terms, reference will now be made to the accompanying drawings, which are not necessarily drawn to scale, and wherein:

FIG. 1 is a perspective view of a medical device introduction system in an embodiment of the present invention;

FIG. 2 is a perspective view of the medical introducer shown in FIG. 1, showing a plug seal in the working channel in an embodiment of the present invention;

FIG. 3 is a view of the medical introducer shown in FIG. 1, showing a plug adapter with seal in the working channel in an embodiment of the present invention;

FIG. 4 is a close-up, perspective view of the manifold of the medical introducer shown in FIG. 1, in an embodiment of the present invention;

FIGS. 18A and 18B are a view of a preformed delivery tube useful in an embodiment of the present invention, showing both assembled and unassembled views;

FIG. 19 is a view of a medical device that has a slider and a rail associated with the medical device;

FIG. 20 is a view of a bent introducer tube;

FIG. 21 is a view of the introducer tube with an accompanying bent sheath;

FIG. 22 is a view of the introducer tube with an accompanying bent sheath wherein distal tip of the introducer tube and the working channel medical device are visible;

FIG. 23 is a view of a uterus wherein the introducer tube is accessing the left osteum and fallopian tube;

FIG. 24 is a view of a uterus wherein the introducer tube is accessing the right osteum and fallopian tube;

FIG. 25 is a view of a manifold wherein the manifold contains a seal that is present at the location of the working channel;

FIGS. 26A and B show an "r" curve and an "s" curve tip, respectively;

FIG. 27 shows an embodiment of the medical introducer device;

FIG. 28 shows a perspective view of the various lumens as they enter into the modular manifold;

FIG. 29 shows a perspective view of the various parts of the modular manifold, the manifold base, the seal and the manifold cover;

FIG. 30 shows the modular manifold in an unassembled state and an assembled state, with the manifold base and the manifold cover separated and then joined;

FIG. 31 shows the modular manifold with lumen core pins as they are used in the process of assembling the modular manifold;

FIG. 32 shows the modular manifold in a vertical position, which shows an embodiment of a process that allows the gluing of the manifold base and the manifold cover (with or without a seal);

FIG. 33 schematically illustrates an imaging system adapted for use with a medical device introduction system, according to various aspects of the present disclosure;

FIG. 34 schematically illustrates a cross-section of a flexible elongate tubular member adapted for use with a medical device introduction system, according to various aspects of the present disclosure;

FIG. 35 schematically illustrates a cross-section of a flexible elongate tubular member having an imaging device mounted therein, and adapted for use with a medical device introduction system, according to various aspects of the present disclosure;

FIG. 36 schematically illustrates a medical device introduction system, according to another aspect of the present disclosure;

FIG. 37 schematically illustrates a disassembled medical device introduction system, according to the aspect of the disclosure shown in FIG. 36;

FIG. 38 schematically illustrates a disassembled medical imager capable of being used in a medical device introduction system, according to the aspect of the disclosure shown in FIG. 36;

FIG. 39 schematically illustrates a medical introducer and the interaction thereof with a tube sheath, both

desired for purposes such as adjusting the starting position of the steerable working channel tube 42 prior to extending or deflecting the distal tip of the working channel tube 42, or reorienting fluid outflow at a target area in the interior body region. In this manner, the true movement of the medical introducer 20 relative to a certain starting point can be gauged. Likewise, if desired, the medical introducer 20 and the attached steerable working channel device 40 can be held in a constant position so as to maintain a fixed orientation, or reference point, of the working channel tube 42 and the working channel in the interior body region. While the medical introducer 20 and the attached steerable working channel device 40 can be held in a constant position, the position of imaging system 60 can be adjusted. In this manner, the true movement of the imaging system 60 relative to a certain starting point can be gauged.

This combination of separate and cooperating components of embodiments of the present invention allows for more precise control of instrument positioning and delivery of materials, such as fluids, medications, and implants, in an interior body region. Independent position control and movement of the imaging system 60 relative to the medical introducer 20 and to the steerable working channel device 40 allows optimal visualization of a target operative site within an interior body region.

An embodiment of the medical device introduction system 10 of the present invention can include a medical introducer 20. As used herein, a "medical introducer" is defined as an instrument used to introduce a medical device, for example, a tube, stent, catheter, and/or surgical instrument, into an interior body region of a human or animal.

In some embodiments of the present invention, the medical introducer device 20 can include the handle 21 comprising an oval-shaped ring of material having an open interior, a proximal end, and a distal end. The introducer 20 can further include an elongate introducer tube 23 extending from the distal end 15 of the handle 21 and having a plurality of lumens extending longitudinally therein. The proximal end 14 of the handle 21 can be configured to receive at least one fluid tube 24, 25 and the imaging system 60 through the handle 21. The distal end 15 of the handle 21 can be adapted to connect to the introducer tube 23, as described herein. Such a medical introducer 20 can be inserted into an interior body region of a patient.

The plurality of lumens in a medical introducer tube 23 can include a scope lumen 34, at least one working lumen 35, and at least one fluid lumen 36 separate from the scope lumen 34 and the working lumen(s) 35. The medical introducer 20 can further include a fluid inflow tube 24 routed through the proximal end of the handle 21 and in fluid communication with one of the at least one fluid lumen 36. The medical introducer 20 can further include the fluid outflow tube 25 routed through the proximal end of the handle 21 and in fluid communication with another one of the fluid lumen(s) 36. In certain embodiments, the diameter of the working lumen 35 can be larger than the diameter of the other lumens 34, 36.

In an embodiment, the working lumen 35 can accommodate medical devices, which can place medications and/or provide implants to an interior body region. However, these medical devices sometimes need to be removed and/or resubmitted. When this occurs, there is the danger of backflow from fluids from the interior body region. Accordingly, in one embodiment, the medical devices of the present invention also possess a manifold 250 and seal 251 as shown in FIG. 25, which will aid ameliorating, diminishing and/or eliminating the backflow of fluids. It should be noted the similarities between FIG. 25 and for example, FIG. 13, wherein the manifold 250 is designed in a way to accommodate the various lumens as shown in FIG. 13. Note that the working lumen 35 is the one that may have medical devices inserted and removed so the manifold 250 contains the seal 251 in the position that is designed to accommodate these medical devices. The seal 251 in some embodiments has flaps associated with it that allow the passage of the medical device but preclude the passage of fluid one the medical device has been removed. The manifold 250 may be made of a plastic that provides the medical device with additional structural integrity that might not otherwise be present.

The medical introducer 20 can be utilized to perform diagnostic procedures, for example, by using the dedicated fluid-in and fluid-out lumens 36 and tubes 24, 25, respectively, to irrigate an interior body region and retrieve a sampling of washings from the targeted region for diagnostic tests. Alternatively, or in addition, the medical introducer 20 can be utilized to perform therapeutic procedures, for example, by using the dedicated working lumen 35 to introduce a device for placing a medication and/or an implant into an interior body region.

The fluid-in tube 24 can include a pinch clamp 26 for on-off regulation of fluid delivery into the interior

In some embodiments, the introducer handle 21 can have a size adapted to be readily held in a hand of a user. In some embodiments, the introducer handle 21 can further include a plurality of raised grips 32 on an outside surface of the handle 21 to assist in manipulating the handle 21.

Embodiments of the medical introducer 20 can have varied numbers, sizes, and configurations of lumens 34, 35, 36 in the introducer 20. Embodiments of the medical introducer 20 can have various lengths, depending on the particular interior body region it is designed to access and on the particular medical procedure for which it is designed. For example, in some embodiments, the medical introducer 20 can include a 7 French size dedicated working lumen 35 so as to support passage of larger devices than conventional multiple lumen delivery devices having the same outside diameter. This advantage is provided by having a smaller dedicated scope lumen 34 and extruding the manifold 22 and introducer tube 23 with smaller wall thicknesses.

In certain embodiments, the introducer handle 21 can include a scope connector 28 located on the proximal end 14 of the handle 21. The scope connector 28 can be longitudinally aligned with the one of the plurality of lumens 34 in the introducer tube 23. The imaging system 60 can be securely connected to the scope connector 28, for example, with a luer lock fitting. When the imaging system 60 is securely connected to the scope connector 28, the imaging system 60--medical introducer 20 interface is adapted to allow the imaging system 60 to rotate independent of movement of movement of the medical introducer 20.

The medical introducer 20 can be formed in a molding process by a plastic or polymeric material. The medical introducer 20 can be formed from materials and in such a manner so as to have most, or all, components be translucent, thereby enabling visualization and visually-guided passage of instruments and fluids through the introducer 20. Such visualization may also assist with establishing delivery routes as discussed herein. Further, such visualization may allow for the identification of a gaseous material (e.g. air) within a channel, and/or confirmation of the absence of such gaseous material within a channel.

The lumen 35 in the medical introducer 20 designed for inserting the steerable working channel device 40 can be sealed with a sealing mechanism. Such a seal 37 can be a duckbill seal or a one-way valve, including a luer fitting. The seals 37 can provide frictional or abutting contact with the inner surface of the working lumen 35 in the manifold 22. Such a seal 37 mechanism can allow medical devices and/or fluid, for example, gas or liquid, to pass through the seal mechanism 37 toward the distal end of the introducer tube 23, and can inhibit fluid from passing from the interior body region through the proximal end 11 of the introducer tube 23.

In certain embodiments, the medical introducer 20 can be inserted into an interior body region with a trocar system (not shown). A trocar can comprise a cannula that may have a sharp distal tip for creating a percutaneous path to the interior body region. Once the trocar is in a desired position in or adjacent the target interior body region, the medical introducer 20 can be inserted through the trocar to the target site. In such an application, a portion of the patient's body needs to be penetrated or opened where a body cavity does not provide a ready opening. Such a trocar system can be used, for example, for prostate surgery. In this manner, a trocar system, or other endoscopic device, can assist in providing a path through which the medical introducer 20 can enter the portion of the interior body region of a patient into which a medical procedure is desired to be performed.

The medical introducer 20 can be utilized to perform diagnostic procedures, for example, by using the dedicated fluid-in and fluid-out lumens 36 and tubes 24, 25 to irrigate an interior body region and retrieve a sampling of washings from the targeted region. Alternatively, or in addition, the medical introducer 20 can be utilized to perform therapeutic procedures, for example, by using the dedicated working lumen 35 to introduce a device for placing an implant into an interior body region.

In an alternative embodiment, the medical introducer 20 can further include an inflatable portion associated with the distal portion of the introducer tube 23. The inflatable portion can be utilized to distend or enlarge a cavity, space, or portion of an interior body region and/or block fluid passage from the interior body region when the introducer tube 23 is positioned therein.

In another aspect of the present invention, some embodiments can include a working channel device 40 that is steerable. The entire length of the working channel tube 42 can be flexible. Alternatively, a substantial portion of the working channel tube 42 can be generally rigid, or semi-rigid, and a distal portion 12 of the

implants, or other materials into an interior body region. The steerable working channel device 40 can be positioned in at least one other of the plurality of lumen 35 of the medical introducer 20 so that the separate steerable working channel device 40 and the imaging system 60 are independently controllable. In some embodiments, the working channel device 40 can be disposable and intended for a single use.

An example of an embodiment of a flexible distal portion 12 and steering wire configuration is shown in FIG. 12. In this embodiment, the working channel tube of the steerable working channel device 40 can comprise a proximal 11 insertion portion, a distal portion 12, and a distal tip 13. The proximal 11 insertion portion can be formed of a semi-rigid material 67, for example, pellethane having a 75 durometer hardness rating. The distal portion 12 can be formed of a combination of a relatively harder material 67, such as a 75 durometer pellethane, and a relatively softer, flexible material 68, such as pellethane having a 55 durometer. The portion of the distal portion 12 having different relative hardness can be co-extruded. The distal tip 13 can be formed of a semi-rigid material 67, which can be the same material from which the proximal 11 insertion portion is formed (for example, pellethane having a 75 durometer). In certain embodiments, other materials can be used to form the elongate tube 42 of the steerable working channel device 40.

The working channel tube 42 can include at least one steering lumen 66 in each lateral aspect of the tube 42. The steering wires can be routed from the position controller 41 through the steering wire lumens 66 through the flexible distal portion 12 and attached to the distal tip 13. The distal tip 13 is preferably formed of a harder material 67, such as a 75 durometer Pellethane, to provide a strong and firm anchor for the small diameter stainless steel steering wires that may cut through a softer material 68 when retracted. The flexible distal portion 12 can include a relatively softer material 68 in each of the lateral aspects through which the steering wire lumens 66 are formed, and a relatively harder material 67 in the dorsal and ventral aspects of the distal portion 12 tubing. Such a configuration can permit the distal portion 12 to deflect in a predetermined manner and amount. The presence of the relatively harder material 67 in the distal portion 12 allows the relatively softer, lateral sections 68 to deflect without compressing when extreme deflection is occurring, which can result in exposing an instrument in the steerable working channel more than desired. Different relative durometers of material can be utilized to achieve a relative hardness/softness ratio between sections of the distal portion 12 so as to allow directionally-controlled deflection of the distal portion 12 of the working channel tube 42.

When the position controller upper housing portion 50 is rotated, one of the steering wires connected to the rotor 55 is wound about the rotor 55, causing the distal end of that steering wire to retract. This retraction pulls on the lateral side of the distal tip of the working channel tube 42 to which it is connected so as to "deflect" the distal tip and distal portion 12 at an angle 57 laterally away from the longitudinal axis 33 of the working channel tube 42, as shown in FIGS. 9 and 10. The position controller upper housing 50 can be rotated in the opposite direction to place tension on, or retract, the other steering wire and thereby "deflect" the distal portion 12 of the working channel tube 42 in the opposite direction. The position controller 41 can thus control the angular attitude of the distal portion 12 of the working channel tube 42. The steering wires in cooperation with the position controller 41 can be configured to limit angular adjustments of the distal portion 12 to a plane extending generally parallel to the upper surface of the position controller 41. For example, the configuration of the position controller 41 and the steering wires can be such that angular deflection 57 of the distal portion 12 of the working channel tube 42 can be limited to no more than 30 degrees, 45 degrees, or another predetermined limit. In other embodiments, various other steering mechanisms, such as one or more position deflectors associated with the working channel tube 42, can be used in accordance with the present invention.

In some embodiments, the position controller 41 can include a braking mechanism (not shown) for securing the upper and lower housing portions 50, 51, respectively, into position relative to each other. The braking mechanism can comprise, for example, a soft polymeric material, such as silicone, coated onto the outer surface(s) of the upper housing rotor 55 and/or the lower housing hub 54. In this fashion, the coated surface can allow the rotor 55 to rotate smoothly within the hub 54, while providing sufficient friction to hold the rotor 55 and the hub 54 of the upper and lower housings 50, 51, respectively, in position when released by an operator. In certain embodiments, in addition to providing a polymeric coating on the rotor 55 and/or hub 54 outer surfaces, one or both of these surfaces can be textured so as to provide further friction and greater securing force between the rotor 55 and hub 54. Such a braking mechanism is simple, inexpensive, and avoids any need for stronger mechanical or gear-based braking mechanisms. In particular embodiments, such a polymeric coating braking mechanism can be combined with other braking means.

is, culdoscopy, transvaginal hydro laparoscopy), and/or falloscopy. Accordingly, both fluid management and medical instruments usage may be managed through the working channel device 40 independent of or separate from both the imaging system 60 and the medical introducer 20.

In certain embodiments, the separate working channel device 40--insertable through a separate lumen 35 in the medical introducer 20 from the lumen 34 in which the imaging system 60 is inserted--can be a non-steerable working channel device 40. In such an embodiment, the working channel device does not have a steering mechanism associated with the device 40. However, the non-steerable working channel device can be moved in the distal and proximal directions within one of the lumen 35 of the medical introducer 20.

In some embodiments of the separate working channel device 40, the proximal end 11 of the working channel tube 42 can include one or more access ports 38, as shown in FIGS. 1 and 6. Such access ports 38 can be sealed with a port seal 39. Such a seal 39 can be formed of an elastomeric material such as silicone rubber and have a very small axial opening through the material that permits a small object such as a needle to enter, but which otherwise prevents fluid flow in either direction, and thus protects the lumens from receiving contaminating materials therein, in some embodiments, the proximal access 38 on the working channel tube 42 can comprise a luer lock fitting and seal 44 for controllable access to the steerable working channel.

In some embodiments, the imaging system 60 can include an endoscopic cannula 62, a light delivery mechanism, and an imaging device. The imaging system can include at least one of an optical scope, an ultrasound instrument, and/or a camera 61. A camera may be positioned on a distal 12 portion of the endoscopic cannula 62.

In some embodiments, the introducer handle 21 can further include a scope connector 28 located on an opposite side of the handle 21 from the introducer tube 23 and longitudinally aligned with the one 34 of the plurality of lumens in the introducer tube 23. In this manner the imaging system 60 can be securely connected to the scope connector 28. In this configuration, that is, when the imaging system 60 is securely connected to the scope connector 28, the imaging system 60 can rotate independent of movement of the medical introducer 20.

In some embodiments, the endoscopic cannula, or endoscope, 62 can be rigid. In other embodiments, the endoscope 62 can be flexible. An embodiment of a flexible endoscopic cannula 62 can include a proximal 11 portion having a first durometer and a distal 12 portion having a second durometer. The second durometer is lower than the first durometer, which can allow deflection of the distal portion 12 for improved viewing of a target area in the interior body region. Some embodiments of the imaging system 60 can further include at least two steering wires (not shown), each wire having its distal end connected to the distal tip 13 of the endoscopic cannula 62. The steering wires can extend at least the length of the endoscopic cannula 62. The proximal end of the steering wires can be operably connected to a deflection control mechanism at the proximal end 11 of the endoscopic cannula 62. In this way, actuation of the deflection control mechanism can cause the distal tip 13 of the endoscopic cannula 62 to deflect at an angle away from the longitudinal axis 33 of the imaging system 60. The endoscopic cannula 62 can include each of a first pair of wires adjacent opposite points on a circumference of the endoscopic cannula 62 to deflect the distal tip along a first axis. The endoscopic cannula 62 can also include each of a second pair of wires adjacent two other opposite points on the circumference of the endoscopic cannula 62. Each of the second pair of wires can be positioned 90 degrees from each of the first pair of wires, to deflect the distal tip along a second axis perpendicular to the first axis.

In some embodiments, the light delivery mechanism can include one or more light emitting diodes (not shown) mounted at a distal tip of the endoscopic cannula 62. In other embodiments, the light delivery mechanism can include a plurality of light delivery fibers (not shown) attached to the endoscopic cannula 62 and extending from the proximal end 11 to the distal tip 13 of the endoscopic cannula 62. The light delivery mechanism can further include a light source (not shown) comprising a light cable attached on one end to a power source and on the opposite end to the light delivery fibers at the proximal end 11 of the endoscopic cannula 62. Alternatively, the light delivery mechanism can further include a light source comprising one or more light emitting diodes connected to the light delivery fibers at the proximal end 11 of the endoscopic cannula 62. In another embodiment, the light delivery mechanism can include a plurality of light delivery fibers integrated into the endoscopic cannula 62 that extend from the proximal end 11 to the distal tip 13 of

the endoscopic cannula 62. In this embodiment, the light delivery mechanism can further include a light source comprising a light cable attached on one end to a power source and on the opposite end to the light delivery fibers at the proximal end 11 of the endoscopic cannula 62. Alternatively, the light delivery mechanism can further include a light source comprising light emitting diodes in the introducer handle connected, to the light delivery fibers.

In some embodiments, the medical device introduction system 10 of the present invention can include an imaging system 60. The imaging system 60 can be separate from the medical introducer 20, and can be positioned in a predetermined one 34 of the plurality of lumens of the medical introducer 20, for example, in the dedicated scope lumen 34. The scope lumen 34 can be configured to receive various types of imaging systems 60 therein. The imaging system 60 can be removably connected to the medical introducer 20.

As described herein, in various embodiments of the medical device introduction system 10, the imaging system 60 can be operated independent of the medical introducer 20 and/or the working channel device 40, thereby permitting a steady, or constant, view of a particular anatomical structure or site in an interior body region while the introducer 20 and/or the working channel device 40 are manipulated. Such an independent operation of the imaging system 60 can be accomplished, for example, through cooperation of the imaging system 60 with the scope port, or connector, 28 as shown in FIGS. 1-3.

The scope connector 28 is fixed to, for example, by being integrally molded with, the proximal end 14 of the medical introducer handle 21. The scope connector 28 can be positioned in longitudinal alignment with the dedicated scope lumen 34 in the introducer manifold 22. The scope connector 28 can include a molded luer lock fitting, which allows the scope 62 to be securely connected to the introducer handle 21, and to also rotate about its longitudinal axis 33 independent from movement of the medical introducer 20. In an application in which the scope 62 is not secured to the introducer handle 21, the imaging system 60 can also be rotated about its longitudinal axis 33 independent from movement of the medical introducer 20. In this way, the medical introducer 20 and/or the working channel device 40 associated therewith can be moved without moving the imaging system 60. As a result, the view through the imaging system 60 can remain constant, providing a fixed reference point for movement of the introducer 20 and/or working channel device 40, and thereby allowing the physician to maintain a steady, right-side-up orientation of view and movement in the interior body region.

The imaging system 60 can comprise, for example, an optical scope, such as a fiber optic scope, a camera 61, a charge couple device (CCD), a camera positioned on the distal tip 13 and/or distal portion 12 of an elongate shaft 62, known as a "chip-on-a-stick," or ultrasound or other sonic device. The imaging system 60 can include a light source (not shown) for illuminating an interior body region. The light source can be separate from, and removably connected to, the imaging system 60. Alternatively, the light source can be integrated with the imaging system 60. As shown in the embodiment in FIGS. 1, 3, and 11, the imaging system 60 can include a fiberscope 62 operably connected to an ocular mechanism, such as an endoscope lens 63, to adjust focus or light intensity. The fiberscope 62 can be, for example, a 2.0 mm 50 K fiberscope, and the endoscope lens 63 can be a 2.9 mm 30 degree rod lens. As shown in this embodiment, the imaging system 60 can be a "low profile" camera 61, which is less bulky, weighs less, and more easily maneuverable than other cameras, and is configured to readily cooperate with other components of the medical device introduction system 10.

The imaging system 60 can be connected to a monitor or other display mechanism for viewing an image within at least a portion of the interior body region into which the imaging system 60 is inserted. The imaging system 60 can be connected to an image capture mechanism, for example, a computer-readable medium such as a computer hard drive, a memory stick, a compact disc, a digital versatile disc, magnetic tape, or other storage medium, for recording images viewed via the imaging device.

In another aspect of the present disclosure, as shown, for example, in FIG. 33, the imaging system 60 may comprise a body member 400 including a light source 425 configured to emit light. A flexible elongate tubular member 450 has a proximal portion 450A operably engaged with the body member 400, and extends to an opposed distal portion 450B. An imaging device 475 (see, e.g., FIG. 35) is engaged with the distal portion 450B of the tubular member 450 and is configured to be in communication with the body member 400. The imaging device 475 is arranged with respect to the distal portion 450B of the tubular member 450 so as to be directed, and to be capable of capturing an image, in an imaging direction 480 outwardly of the distal portion 450B. A plurality of light transmission devices 500 is operably engaged with and extends from

the light source 425 and through the tubular member 450 to respective distal ends 505 thereof disposed about the distal portion 450B of the tubular member 450. The light transmission devices 500 are configured to receive the light from the light source 425 and to transmit the light to the distal ends thereof 505, such that the light is emitted from the distal ends 505. The distal ends 505 of the light transmission devices 500 are arranged about the imaging device 475, about the distal portion 450B of the tubular member 450, so as to direct the light transmitted from the light source 425 in the imaging direction 480, outwardly of the distal portion 450B of the tubular member 450.

In some instances, the flexible elongate tubular member 450 may comprise, for example, a braided elastic filiform material configured to transmit torque between the proximal and distal portions 450A, 450B of the tubular member 450. The braided elastic filiform material may comprise, for instance, a stainless steel braided sleeve or hose, though a braided filiform material of various types could also be used (i.e., by varying the arrangement of the braiding or weaving) to provide desirable characteristics in terms of the ability to transmit torque, while maintaining the desirable flexibility of the tubular member 450 along the length thereof. The tubular member 450 is preferably sufficiently flexible, at least about the distal portion 450B thereof, to conform to the curvature of the distal portion 12 of the introducer tube 23, as disclosed elsewhere herein. In other instances, if necessary or desired, a rigid elongate conduit 440 may be engaged between the body member 400 and the flexible elongate tubular member 450 so as to be capable of transmitting torque between the body member 400 and the flexible elongate tubular member 450. In still other instances, if necessary or desired, the rigid elongate conduit 440 may extend over the flexible elongate tubular member 450 about the engagement thereof with the body member 400. In further instances, the tubular member 450 may comprise an external polymeric sheath 460 disposed externally to the braided filiform material 455 and/or an internal polymeric sheath 465 disposed internally to the braided filiform material 455 (see, e.g., FIG. 34). Such polymeric sheaths 460, 465 may comprise separate and discrete tubes that may be coaxially arranged with the braided filiform material 455. In other instances, the polymeric sheaths 460, 465 may be engaged with the braided filiform material, for example, in a co-extrusion or coating process. In some instances, as further disclosed herein, the tubular member 450 may be employed to carry a plurality of light transmission devices (i.e., light delivery fibers) therein and, as such, it may be desirable for the external and/or internal polymeric sheaths 460, 465 to be opaque to preserve the light transmitted by the light transmission devices 500 through the distal ends 505 thereof.

In some aspects, the tubular member 450 may further comprise a terminal member 525 engaged with the braided filiform material 455 about the distal portion 450B of the tubular member 450. That is, termination of the braided filiform material 455 may result in loose/protruding filaments of the braided material. Accordingly, the terminal member 525 may be applied to cap or seal the terminus of the braided filiform material 455, for instance, to prevent such loose/protruding filaments. However, the terminal member 525 may also be configured to receive and secure the imaging device 475 and/or the distal ends 505 of the light transmission devices 500.

In one aspect, the light transmission devices 500 may comprise fiber optic elements or light delivery fibers. In another aspect, the imaging device 475 may comprise an active-pixel sensor array or a Complementary Metal-Oxide Semiconductor (CMOS) sensor. It may be desirable, in some instances, for the imaging device 475 to capture images substantially in real time or at least with minimal delay between image capture and display. In such aspects, the imaging device 475 may be configured as a quadrilateral, generally configured to be received within a lumen defined by an inner wall (i.e., the braided filiform material 455 or the internal polymeric sheath 465) of the tubular member 450. In such instances, it may be preferable that the imaging device 475 be received and arranged so as to be disposed perpendicularly to a longitudinal axis of the tubular member 450 (i.e., the longitudinal axis of the tubular member 450 extends perpendicularly through the plane of the imaging device 475). Further, in general, the lumen defined by the tubular member 450 has a non-polygonal cross-section. That is, the lumen defined by the tubular member 450 may be configured to have, for example, a circular, oval, or ovate cross-section. In some particular instances, the imaging device 475 may be configured as a square (i.e., having a diagonal dimension of about 2.3 mm), and is received within a lumen configured to have a circular cross-section having, for example, an inner diameter of about 2.3 mm (see, e.g., FIG. 35), and the light transmission devices 500 may comprise fiber optic elements or light delivery fibers having the distal ends 505 thereof arranged about the imaging device 475 in the segments of the circular lumen unoccupied by the imaging device 475. In such a configuration, the unoccupied segments about the imaging device 475 may each include the distal ends 505 of a plurality of fiber optic elements or light delivery fibers. In this manner, significant illumination may be directed from the distal ends of the light

can allow a physician to utilize embodiments of the present invention to perform procedures in an office setting which may have previously been avoided due to complexity and cost.

In particular, the ability to maintain a constant, or fixed, point of reference, for example, by keeping the imaging system 60 steady while re-positioning the medical introducer 20 and/or the working channel device(s) 40 can provide greater control over the medical procedure, and may decrease operative time. Embodiments of medical device introduction systems 10, devices 20, kits, and methods of the present invention can be utilized in conjunction with procedures that are minimally invasive. Whether used alone or in the context of minimally invasive procedures embodiments of the present invention can advantageously provide, for example, performing the procedure on an outpatient basis, reduced trauma to the target area, reduced anesthesia time, reduced recovery time, and decreased discomfort to the patient. As an example, in a hysteroscopy system, an embodiment of the present invention can allow a fixed endoscope 62 position, thereby minimizing tissue trauma as compared to conventional hysteroscopy procedures. In addition, minimal outside diameters of the medical introducer 20 and associated components resulting in smaller devices can decrease the need for anesthesia and can increase patient comfort related to a procedure.

Single use components can be safer than reusable devices due to the decrease or elimination of risk for transmission of communicable infections and diseases between patients. Single use components can be more cost-effective due to elimination of cleaning and sterilization expense and decreased expense for repairs associated with reusable devices.

In another aspect of the present invention, certain embodiments of the medical introducer 20 can further include a lift wire (not shown) attached on its proximal end to a distal tip lift control (not shown), such as a knob similar to the steerable working channel device position controller 41. The lift wire can be routed through a dedicated lift wire lumen 69, as shown in FIG. 13, through the length of the medical introducer tube 23 and attached on its distal end to the distal tip 13 of the introducer tube 23. The distal lift control can be moved in the proximal direction so as to pull the lift wire in the proximal direction, thereby deflecting the distal tip 13 of the introducer tube 23 in one direction. When the distal tip 13 of the introducer tube 23 is lifted, any device therein will also be lifted, or deflected, along with the introducer tube 20. In operation, the introducer tube 20 can be inserted in the straight position (along its longitudinal axis).

In an exemplary embodiment, a flexible medical device, such as a flexible hysteroscope, can be inserted in the working channel, or lumen, 35 of the medical introducer 20. Once the introducer tube 23 is inserted in the straight position into the uterine cavity 64 (FIG. 10) and the cavity 64 distended, the distal tip lift control can be moved in the proximal direction so as to lift the distal tip of the introducer tube 23 in one direction. The introducer 20 can then be rotated to view the extreme left and right aspects of the uterine cavity 64. The distal tip of the introducer tube 23 can be further positioned and aligned with the tubal ostium for delivery of an instrument or implant to the fallopian tube 65. Such an embodiment can thus provide a simple operation for lifting, or deflecting, a steerable working channel device 40, imaging system 60, or other medical device in an interior body region.

Some embodiments of a medical device introduction system 10 of the present invention can include an accessory device support 70, as shown in FIG. 15. The accessory device support 70 can be removably connected to the introducer handle 21. The accessory device support 70 can comprise a carrier arm 72 for supporting an upper part of a body of a separate medical device 73 to be used with the medical introducer 20, and a slide member (or mechanism) 71 for slidably supporting a lower part of the body of the separate medical device 73. This accessory device support 70 can be used to stabilize placement of additional separate medical devices (73) in the interior body region. In certain embodiments, the accessory device support 70 can be removably connected to the outside surface of the scope connector 28 on the proximal end of the introducer handle 21.

An embodiment of the present invention can include a delivery catheter having a small delivery channel, or working lumen 35, as shown in FIG. 14. Such a configuration allows the scope lumen 34 to be larger than, for example, the embodiment shown in FIG. 5. In the embodiment shown in FIG. 14, the catheter can be inserted into the interior body region in the straight position. For example, a flexible hysteroscope can be introduced into the uterine cavity 64 in the straight position via a small delivery catheter. Once inserted, and the cavity 64 is distended, the medical introducer 20 can be rotated to provide an optimal viewing angle. The flexible hysteroscope can have a pre-formed "angle up" distal tip 13, and can be inserted via the working

delivery channel in an obturator. Once in the uterine cavity 64, the obturator can be removed, and the angled distal tip is restored for use. This enables a zero degree angle of view flexible scope to be utilized and a more effective access approach to particular pathologies. Such a small diameter delivery catheter can assist visualization and access in difficult to reach pathology. In addition, a small diameter catheter can improve patient comfort relative to larger delivery catheters.

As shown in FIG. 16, an embodiment of the present invention can include a continuous flow examination sheath 80. This device 80 can be single-use and utilized for quick evaluation or hysteroscopy, for example. The continuous flow examination sheath 80 can include a formed distal tip 81, an insertion portion 82, a fluid-out adapter 84, a fluid-in adapter 83, a finger grip 85, a proximal port 86, and an inner sheath 87. An endoscope 62 can be inserted through the proximal port 86 through a fluid seal adapter (not shown). The fluid-in tube 83 can allow a physician to deliver fluid to clear the scope 62 lens or distend the uterine cavity 64 for improved visualization. In addition, the fluid-out adapter 84, and tube, can allow the physician to clear fluid from the cavity 64 that may impair viewing caused by blood present at the site.

As shown in FIG. 17, an embodiment of the present invention can include a single flow examination sheath 90. This device 90 can be single-use and utilized for quick evaluation or hysteroscopy, for example. The single flow examination sheath 90 can include a formed distal tip 81, an insertion portion 82, a fluid-in adapter 83, a finger grip 85, a proximal port 86, and a nose piece 91. An endoscope 62 can be inserted through the proximal port 86 through a fluid seal adapter. The fluid-in tube 83 can allow a physician to deliver fluid to clear the scope lens or distend the uterine cavity 64 for improved visualization.

As shown in FIG. 18, an embodiment of the present invention can include a pre-formed delivery catheter 100. The pre-formed delivery catheter 100 can include a formed distal tip 81, an insertion portion 82, an adapter 101, a finger grip 85, a proximal port 86, and a nose piece 91. This device 100 can be used for delivering another medical device or treatment to a specific site when a steerable mechanism is not practical. Fluid can be incorporated by adapters known in the art, for example, a Touhy Borst adapter and a side port entry attached to the proximal end of the catheter 100.

In another embodiment, an endoscopy system utilized in the present invention can be a wireless handheld endoscopy system (not shown). Such a system can include an endoscopic cannula 62, a disposable mount, a focus/zoom function, a wireless camera, for example, a 2.4 GHz, high resolution camera used in cooperation with a laptop or other monitor, and controls for imaging and power.

Some embodiments of a medical device introduction system 10 can be utilized with a conventional endoscope trocar system (not shown), for example, for abdominal minimally invasive surgery. The medical introducer 20 can be inserted through a 10 mm or 5 mm trocar and can be sealed by the internal trocar seal. When inserted with a conventional trocar system, embodiments of the present invention can retain all functionality described herein, including depth adjustment for the medical introducer 20, 360 degrees of rotation, depth adjustment for the steerable working channel device 40, and angle and direction of deflection adjustment, visualization, and access related to the working channel device 40.

Some embodiments of the present invention can include a kit comprising one or more of various components of a medical device introduction system 10, including a medical introducer 20, a separate imaging system 60, and/or a separate working channel device 40. The medical introducer 20 can include a handle 21 and an elongate introducer tube 23 extending from the distal end 15 of the handle 21. The introducer tube 23 can include a plurality of lumens 34, 35, 36 extending longitudinally therein. The medical introducer 20 may be inserted into an interior body region of a patient. The separate imaging system 60 may be inserted through the handle 21 and positioned in a predetermined one 34 of the plurality of lumens. The imaging system 60 can have an interface with the handle 21 such that each of the imaging system 60 and the medical introducer 20 is movable independent of the other. The separate working channel device 40 can include an working channel tube 42 and a position controller 41. The working channel tube 42 can include at least one lumen extending the length thereof defining a working channel. The position controller 41 can be configured to control positioning of the working channel tube 42. The working channel device 40 may be removably connectable to the handle 21 and positioned in another predetermined one 35 of the plurality of lumens. In some embodiments of a kit of the present invention, each of the medical introducer 20, the imaging system 60, and the working channel device 40 can be movable independent of the other.

thereof defining a working channel. The position controller 41 for controlling the position of the working channel tube 42 can be positioned in the working channel in another predetermined one 35 of the plurality of lumens. In such embodiments, one of the group of the medical introducer 20, the imaging system 60, and the working channel device 40 may be moved independently of the others of the group.

In some embodiments of a method, the medical introducer handle 21 can comprise an oval-shaped ring of material having an open interior. The method can further include connecting a distal end of the handle 21 to the introducer tube 23. In some embodiments of a method, the medical introducer 20 can include a modular manifold 22 integrally formed on a proximal end 11 of the introducer tube 23 and have a corresponding plurality of lumens 34, 35, 36 aligned with the plurality of lumens 34, 35, 36 in the introducer tube 23. In such an embodiment, the manifold 22 can be removably connected to the introducer handle 21. The manifold 22 and introducer tube 23 may be interchanged in the handle 21 with other manifolds 22 and introducer tubes 23.

In an embodiment, a slider 191 and rail 192 may be used in conjunction with a medical device 190 to accommodate the handle of the medical device 190. For example, the slider 191 and rail 192 may be used to accommodate a medical device 190 such as that disclosed in U.S. Pat. No. 8,079,364, which is herein incorporated by reference in its entirety. The rail 192 is designed so as to accommodate the slider 191 so as to serve as a means of holding the medical device 190. In one embodiment, the slider 191 and the rail 190 when serving as a holder of the medical device 190 means that fewer hands are needed in surgery. Without the slider 191 and rail 192, a nurse or some other personnel is needed to hold the medical device 190 to prevent the medical device from turning when inserted into a cavity (for example, into the uterine cavity). Thus, the slider 191 and rail 192 stabilizes the handle without having additional hands having to hold the device.

For example, when a fallopian tube sterilization is performed, often a nurse is required to hold the handle of a medical device 190 while the surgeon operates the device so as to insert an additional medical device or to perform some procedure (such as cauterization or the like). By using the slider 191 and rail 192, the nurse is no longer required to hold the device as the surgeon performing the surgery is able to not only manipulate the distal tip of the medical device to perform the sterilization by inserting the tip through the one or more osteums into the fallopian tube, but is also able to hold the medical device due to the presence of the slider 191 and rail 192. The nurse or other medical personnel is then available to perform other duties (such as helping the anesthesiologist or providing the necessary medical devices to the surgeon).

The uterine cavities in all patients tend to be slightly different. The locations of the osteum may differ slightly from patient to patient meaning that the location of the fallopian tubes may also differ. In one embodiment, the slider 191 and rail 192 may be able to accommodate a medical device 190 that contains a steerable distal tip for a working channel device. The slider 191 and rail 192 in combination with the steerable distal tip allow the surgeon to use a scope to identify the location of the osteum(s) and then to insert a medical device, an example of which is disclosed in U.S. Pat. No. 7,921,848. U.S. Pat. No. 7,921,848 is herein incorporated by reference in its entirety.

In an embodiment, rather than having a steerable distal tip, the distal tip of the medical device may be bent. When performing a female sterilization such as a tubal ligation or a tubal occlusion the bent distal tip may make it easier to access the osteum. Other procedures that can be done include diagnostic hysteroscopy, polypectomy, myomectomy, a directed uterine biopsy, fundal biopsy, endometrial harvesting or tubal patency. See for example, the bent distal tip as shown in FIG. 20. In one embodiment, the angle at which the distal tip is disposed cannot be altered. In other embodiments, the distal tip may be part of the introducer tube that can be bent and thus, altered. When the introducer tube cannot be altered, an osteum (or either of the two ostei) can be accessed by adjusting the distance that the working medical device is inserted into the vagina. When a more acute angle is desired, the surgeon will pull the medical device out more and when a less acute angle is desired, the surgeon will push more of the medical device into the uterus. In any event, by this methodology, the ostei and fallopian tubes can be accessed.

In a variation of this embodiment, the diameter of introducer tube 23 in this embodiment may be less than the diameter of an introducer tube of a medical device that has a steerable distal tip. This is because the working channel medical device no longer requires the mechanism necessary for steering the distal tip. Accordingly, components such as the steering and/or lift wires that are necessary in a steerable working

channel medical device are not required to move the distal tip.

In an alternative embodiment, a sheath that has an inner diameter that is slightly larger than the outer diameter of the working channel medical device may be placed over the distal end of the introducer tube. In several embodiments, the sheath may be bent and may be of sufficient structural integrity so that the sheath also bends the distal end of the medical device to the same degree as the sheath. In one embodiment, a surgeon may use a sheath that is bent at an angle that is 10 degrees from straight. If a scope is associated with the working channel medical device, the surgeon may view the inside of the uterus to ascertain the relative locations of the ostei. There may be other sheaths that are bent at any of a plurality of degrees from straight that can then be inserted over the introducer tube so the appropriate orientation is realized to allow access to the ostei. For example, there may be bent sheaths that may be 10 degrees, 20 degrees, 30 degrees, or 40 degrees from straight. By selecting the correct sheath (after ascertaining the orientation to approach the ostei), the surgeon can most readily perform the procedure in the fallopian tube that is to be performed. An example of the bent sheath can be seen in FIGS. 21 and 22. FIGS. 23 and 24 show the bent sheath with the introducer tube and the working channel medical device approaching the left osteum and left fallopian tube (FIG. 23) and the right osteum and right fallopian tube (FIG. 24). In an embodiment, one might access the right osteum after accessing the left osteum merely by turning the handle 180 degrees (which in turn changes the orientation of the distal tip from accessing the left osteum to being able to access the right osteum or vice versa).

In an embodiment, the present medical device does not rely on the distal tip being correctly oriented by a steerable working channel medical device but rather relies rather on the distal tip of the introducer tube being bent or alternatively, a sheath that fits over the introducer tube that is bent. When the sheath is bent, it has sufficient structural stability so as to bend the distal tip of the working channel medical device. The advantage of these systems is that they require less manipulation at the proximal end of the medical device by the surgeon. The proper orientation is achieved simply by having the correct bend in the introducer tube or the sheath that is designed to accommodate the introducer tube. When the system employing a sheath is used, this system has the advantage that different orientations of the distal tip can be achieved simply by having a plurality of different sheaths that are all bent to slightly different degrees. It should be noted that the orientation may be slightly modified from the plurality of bent sheaths by the relative position of the sheath as it relates to the introducer tube. The closer the sheath is to the proximal end of the medical instrument (closer to the surgeon), the larger the bend of the distal tip end. That is, by having the bend closer to the proximal end, the distal tip will be a further distance from straight.

FIGS. 26A and 26B show two different embodiments of the present invention, the "r" curved embodiment and the "s" curved embodiment, respectively. FIG. 26B shows an introducer with a compound-curved tip 261 that allows the positioning of an imaging device further from an object 262 relative to the simple curve 260. When the introducer is inserted into a small body cavity or vessel, different views of an anatomical site can be attained. The view angle profile of the anatomical site is indicated in both FIGS. 26A and 26B by dotted lines 265 and 265'. Note that because the viewing angles are the same, the further distance 264 of the compound curve relative to the lesser distance 263 of the simple curve allows the user to view more area around the object 262. Nevertheless, in either embodiment, the object 262 to be addressed can be done with steerable working channel 266.

In one embodiment, the compound-curved introducer distal tip (the intersection of dotted lines 265 and 265') is positioned at a distance 264 that is 3-10 mm further from the object 262 (such as an osteum) than a simple curved introducer tip distance 263. The embodiment in FIG. 26B provides more space for the steerable working channel 266 to extend (deploy) out of the distal tip of the introducer and as well as space to be steered (articulated) or deflected within the field of view (265 and 265') of the imaging device and to place in alignment with the tubal osteum to deliver an implant, instrument, energy source, or to perform some therapeutic procedure. The simple-curved device of FIG. 26A provides less working space for a steerable working channel between the introducer distal tip and the object (e.g., the osteum).

In some embodiments, and as shown in FIGS. 27 and 28, the medical introducer 20 can include a modular manifold 271 integrally formed on the proximal end 11 of the introducer tube 23 and having a corresponding plurality of parallel aligned lumens 34, 35, 36 in the introducer tube 23. The manifold can incorporate seal(s) 292 (see FIG. 29) to prevent fluid flow from out of a body cavity or vessel when no instrumentation is in the working channel 35. The seal(s) 290 do(es) not allow fluid or gas flow from a distal position to a proximal

position through specified lumens in the introducer tube 23 but may allow fluid and/or gas to flow in the opposite direction.

The specified lumens in the modular manifold 271 are created by joining a manifold base 291 and a manifold cover 292 (see FIGS. 29 and 30) with the seal 290 (shown in FIG. 29 but not shown in FIG. 30) positioned in the interior of the combined manifold base 291 and manifold cover 292. The manifold base 291, manifold cover 292 and introducer tube 23 can be assembled to form integrally isolated lumens corresponding with the plurality of lumens 34, 35, 36 and introducer tube 23 by aligning the plurality of lumens 34, 35, 36 with sized Teflon core pins 301 (see FIGS. 30 and 31), which hold the relative positions of the plurality of lumens 34, 35, 36 and the introducer tube 23 in place. In an embodiment, one can inject/insert UV curable glue 321 (see FIG. 32) into the assembly at junction 323 between the manifold base 291 and manifold cover 292. The introducer tube 23 with lumen core pins 301 and the modular manifold 271 are all held in a vertical position when inserting the glue (see FIG. 32). The assembly is held in a vertical position so as to allow the passage of the glue by gravity down into the manifold cover 292, which also secures the seal 290 (not shown in FIG. 32) in place. The transparent assembly is subsequently then exposed to UV light to cure the UV glue injected between manifold base 291 and introducer tube 23 contained by cover 292. The core pins 301 can then be removed from the modular manifold 271 containing integral seal(s) 290.

In one embodiment, the seal 290 is situated and is of a type so as to allow the passage of fluid in a direction that is from the proximal end of the introducer medical device to the distal end of the introducer medical device but does not allow passage of fluid in the other direction. In another embodiment, the seal may allow passage of fluid in the other direction. In another embodiment, the seal may prevent passage of fluid at all, or allow only the passage of low viscosity fluids while substantially blocking the passage of medium and/or high viscosity fluids.

In still another aspect of the present disclosure, as shown, for example, in FIGS. 36-40, a medical device introduction system 700 may be adapted to be at least partially insertable into an interior body region of a patient. Such a system 700 may comprise a medical imager 750, a medical introducer 800, and a tube sheath 850. The medical imager 750 may include a body member 755 (see, e.g., element 400 in FIG. 33) being configured as or otherwise including a handle 760, and including a light source (see, e.g., element 425 in FIG. 33) disposed within the handle 760. A flexible elongate tubular member 765 (see, e.g., element 450 and, optionally, element 440, shown in FIG. 33) extends from the body member 755 to an opposed distal portion 770. The tubular member 765 includes an imaging device (see, e.g., element 475 in FIG. 35) engaged with the distal portion 770 thereof. Similarly to the imaging device shown as element 475 in FIG. 35, the imaging device is arranged and configured to be in communication with the body member 755 (i.e., in signal communication with a communication element 550 as shown in FIG. 33). A plurality of light transmission devices (see, e.g., element 500 in FIG. 33) extend from the light source, and through a lumen defined by the tubular member 765, to respective distal ends thereof (see, e.g., elements 505 in FIG. 35) disposed about the distal portion 770 of the tubular member 765, and arranged about the imaging device (see, e.g., FIG. 35). The light transmission devices are configured to receive the light from the light source and to transmit the light to the distal ends thereof.

In particular aspects, the imager 750 is configured similarly to that shown and described in association with FIGS. 33-35. As such, since details of such an imager 750 have already been disclosed herein, such details are not repeated in their entirety in relation to the aspects shown in FIGS. 36-40. In any instance, in light of the previous disclosure herein regarding the imager 750, particular aspects of such an imager 750 will be readily apparent. For example, the light transmission devices (see, e.g., element 500 in FIG. 33) may comprise fiber optic elements or light delivery fibers. In addition, the imaging device (see, e.g., element 475 in FIG. 35) may comprise an active-pixel sensor array or a Complementary Metal-Oxide Semiconductor (CMOS) sensor.

In some aspects, the imaging device (see, e.g., element 475 in FIG. 35) may be configured as a quadrilateral, and is received within a lumen defined by an inner wall of the tubular member 765 of the imager 750, perpendicularly to a longitudinal axis of the tubular member 765, with the lumen being configured to have a circular, oval, or ovate cross-section. In particular aspects, the imaging device (see, e.g., element 475 in FIG. 35) is configured as a square, and is received within a lumen defined by an inner wall of the tubular member 765 of the imager 750, perpendicularly to a longitudinal axis of the tubular member 765, with the lumen being configured to have a circular cross-section. In such instances, the light transmission devices (see, e.g.,

element 500 in FIG. 33), comprising fiber optic elements or light delivery fibers, have the distal ends (see, e.g., element 505 in FIG. 35) thereof arranged about the imaging device (see, e.g., element 475 in FIG. 35) in the segments of the circular lumen unoccupied by the imaging device.

In other aspects, a power source 900 (see, e.g., element 625 in FIG. 33) is operably engaged with the body member (see, e.g., element 400 in FIG. 33), wherein the power source 900 is arranged to be in electrical communication with the light source (see, e.g., element 425 in FIG. 33). The power source 900 may be removably secured to the body member 755, for example, via a magnetic connector arrangement. In addition, a heat shield (see, e.g., element 650 in FIG. 33) may be implemented to wrap about or to surround the power source 900.

In still further aspects, a communication element 950 (see, e.g., element 550 in FIG. 33) may be operably engaged with the body member 755, wherein the communication element 950 is arranged in signal communication with the imaging device (see, e.g., element 475 in FIG. 33) so as to receive an image signal therefrom associated with the image captured thereby or to communicate electrical power to the imaging device. In addition, a display device (see, e.g., element 575 in FIG. 33) for displaying the image, or a computer device (see, e.g., element 600 in FIG. 33) for storing or analyzing the image, may be in communication with the communication element 950 via a wired communication arrangement or a wireless communication arrangement.

In additional aspects, the flexible elongate tubular member 765 may comprise a braided elastic filiform material configured to transmit torque between the proximal and distal portions of the tubular member. In some instances, the tubular member 765 may comprise an external polymeric sheath disposed externally to the braided filiform material, or an internal polymeric sheath disposed internally to the braided filiform material. In particular aspects, the external polymeric sheath and the internal polymeric sheath are opaque to preserve the light transmitted by the light transmission devices (see, e.g., element 500 in FIG. 33). Further, the tubular member 765 may comprise a terminal member (see, e.g., element 525 in FIG. 33) engaged with the braided filiform material about the distal portion 770 of the tubular member 765, wherein the terminal member is configured to receive and secure the imaging device and the distal ends of the light transmission devices.

The medical introducer 800 is comprised of a flexible elongate introducer tube 805 extending from a proximal end 810 to a distal end 815. The introducer tube 805 defines at least one lumen 820 extending longitudinally within the introducer tube 805 from the proximal end 810 to the distal end 815, wherein the lumen 820 is configured to receive the tubular member 765 of the imager 750 therein. More particularly, in some instances, the introducer tube 805 is configured to receive the tubular member 765 of the imager 750 within the lumen 820, such that the imaging device (see, e.g., element 475 in FIG. 35) engaged with the distal end 770 of the tubular member 765 is disposed about the distal end 815 of the introducer tube 805.

In accordance with some aspects of the present disclosure, a transparent member 835 (see, e.g., FIG. 40) may extend across and seal the distal end of the lumen 820 (i.e., about the distal end 815 of the introducer tube 805) configured to receive the tubular member 765 of the imager 750 therein. In such aspects, the distal end 770 of the tubular member 765 is disposed adjacent or in proximity to the transparent member 835, wherein the transparent member 835 is configured to direct light from the light transmission devices (see, e.g., element 500 in FIG. 33) therethrough and/or to allow the imaging device (see, e.g., element 475 in FIG. 35) to receive or capture an image therethrough. Since the lumen 820 is sealed about the distal end 815 of the introducer tube 805, the tubular member 765 of the imager 750 is and will remain isolated with the lumen 820 during use of the medical device introduction system 700. Accordingly, the sealed lumen 820 may facilitate less frequent or no required sterilization of the imager 750 and/or re-usability of the imager 750.

In particular aspects, the introducer tube 805 may define a plurality of lumens (see, e.g., elements 820, 821, 822, and 823 in FIG. 40), with each lumen extending longitudinally within the introducer tube 805 from the proximal end 810 to the distal end 815. That is, as shown in FIG. 40, the introducer tube 805 may define at least four lumens 820, 821, 822, 823, wherein one lumen 821 may comprise a working channel for receiving surgical instruments therethrough. In such instances, an engagement device 830, such as a luer fitting may be engaged about the proximal end 810 of the introducer tube 805 and in communication with the one lumen 821. In this manner, the luer fitting may be configured to engage, secure, and/or form a seal with the surgical instrument inserted into the working channel, with respect to the introducer tube 805. The remaining two

lumens 822, 823 may comprise, for example, fluid in and out channels for directing fluid through one lumen 822 from the proximal end 810 toward the distal end 815 (inflow), and for directing fluid through the other lumen 823 from the distal end 815 toward the proximal end 810 (outflow). As shown, for example, in FIGS. 36 and 37, irrigation inflow and outflow tubes 824, 825 may be engaged and in fluid communication with the lumens 822, 823 arranged and configured a fluid in and out channels, so as to facilitate engagement with fluid/irrigation equipment.

In particular instances, the proximal end 810 of the introducer tube 805 is configured to non-rotatably engage the tubular member 765 or the body member 755 of the imager 750. That is, a securing device 827 may be engaged with the proximal end 810 of the introducer tube 805, and configured to receive the tubular member 765 of the imager 750 therethrough. In some instances, the proximal end 810 of the introducer tube 805 may itself be configured as the securing device 827. In particular instances, the securing device 827 is configured to secure the tubular member 765 with respect to the introducer tube 805 such that the imaging device (see, e.g., element 475 in FIG. 35) is disposed in a selected longitudinal position along the introducer tube 805, and such that the tubular member 765 is non-rotatable about a longitudinal axis thereof within the introducer tube 805. For example, the securing device 827, or otherwise the proximal end 810 of the introducer tube 805 (i.e., at least the lumen 820 configured to receive the tubular member 765 of the imager 750 therein), may define a keyed receptacle (not shown) configured to engage a keyed flange (i.e., element 767 of FIGS. 37 and 38) associated with the tubular member 765 or the body member 755 of the imager 750, in a snap fit or a friction fit, such that the introducer tube 805 is removably and non-rotatably affixed to the tubular member 765 or the body member 755 of the imager 750.

As shown in FIGS. 36, 37, and 39, the elongate tube sheath 850 extends from a proximal end 855 to a distal end 860. The tube sheath 850 may further define a lumen 865 (see, e.g., FIG. 40) configured to receive the introducer tube 805 therein. In particular aspects, the proximal end 855 of the tube sheath 850 is configured to rotatably engage the introducer tube 805 by way of, for example, a rotation element 875 (see, e.g., FIGS. 36, 37, and 39). The rotation element 875 may be configured to engage the introducer tube 805 such that the distal end 815 of the introducer tube 805 (and thus the distal end 770 of the tubular member 765) is disposed at, about, or in proximity to the distal end 860 of the tube sheath 850. That is, in some instances, the tube sheath 850 is configured to receive the introducer tube 805 of the introducer 800 therein such that the distal end 815 thereof is disposed about the distal end 860 of the tube sheath 850, wherein the imaging device (see, e.g., element 475 in FIG. 35) is thereby directed in an imaging direction outwardly of the distal end 860 of the tube sheath 850, and wherein the distal ends (see, e.g., element 505 in FIG. 35) of the light transmission devices (see, e.g., element 500 in FIG. 33) are arranged about the imaging device to direct the light transmitted from the light source (see, e.g., element 425 in FIG. 33) in the imaging direction.

In some aspects, at least the distal ends 770, 815 of the tubular member 765 of the imager 750 and the introducer tube 805 of the introducer 800 are configured to be flexible. Further, at least the distal end 860 of the tube sheath 850 may be configured to be relatively rigid, at least compared to the distal ends 770, 815 of the tubular member 765 of the imager 750 and the introducer tube 805 of the introducer 800. In addition, at least the distal end 860 of the tube sheath 850 may be configured as a curve or a compound curve (see, e.g., FIGS. 36, 37, and 39). Accordingly, at least the distal ends 770, 815 of the tubular member 765 of the imager 750 and the introducer tube 805 of the introducer 800 will flex during longitudinal movement of the introducer tube 805 within the tube sheath 850, or longitudinal movement of the tubular member 765 of the imager 750 within the lumen 820 defined by the introducer tube 805 of the introducer 800, so as to conform to the curve or the compound curve of the distal end 860 of the tube sheath 850.

As such, for example, by a user grasping the body member 755 of the imager 750 in one hand, and the rotation element 875 associated with the tube sheath 850 in the other hand, the tube sheath 850 can be rotated with respect to the introducer tube 805/tubular member 765. In response, at least the distal ends 770, 815 of the tubular member 765 of the imager 750 and the introducer tube 805 of the introducer 800 will continue to conform to the distal end 860 of the tube sheath 850, upon rotation thereof (see, e.g., FIG. 39), and will therefore rotate, orbit, or gyrate about the longitudinal axis of the tube sheath 850 as directed by the curve or compound curve. Since, in such an arrangement, the imaging device (see, e.g., element 475 in FIG. 35) is directed outwardly of the distal end 860 of the tube sheath 850, due to the relation between the distal end 860 of the tube sheath 850 and at least the distal ends 770, 815 of the tubular member 765 of the imager 750 and the introducer tube 805 of the introducer 800, the imaging direction of the imaging device is altered in response to the rotation of the tube sheath 850 about the introducer tube 805. Accordingly, the imaging

device (see, e.g., element 475 in FIG. 35) may be readily and accurately steered in regard to the particular imaging direction by merely rotating the tube sheath 850 about the introducer tube 805, without otherwise requiring a separate steering arrangement.

Certain embodiments of a method of the present invention include performing a medical procedure in an interior body region through the working channel device 40. For example, the medical procedure can be a gynecological procedure, a spinal procedure, or other procedure.

In some embodiments, a kit comprises at least one of a medical introducer; an imaging device; or a working channel device. In some embodiments a kit comprises a medical introducer and a working channel device. In some embodiment a kit comprises a working channel device inserted into a medical introducer.

The devices, systems, kits, and methods embodying the present invention can be adapted for use in many suitable interior body regions in humans and animals, wherever it may be desirable to provide support for a tissue. The illustrative embodiments are described in association with devices, systems, kits, and methods used, to access interior body regions such as the uterine cavity 64. For example, the medical device introduction system 10, and, in particular, the cooperating medical introducer 20, steerable working channel device 40, and imaging system 60 can be utilized to perform a hysteroscopy.

FIGS. 41 through 43 illustrate a more refined version of the system disclosed herein. As illustrated, rotation element 875 is rotated in order to impart rotation to tube sheath 850, which then imparts movement to the scope enclosed therein that has already been described herein. FIGS. 42 and 43 illustrate various scope and lumen arrangements provided herein.

FIG. 44 illustrates a system 900 with an introducer 904 with a sheath 902 located inside the scope lumen 906. The sheath may be a urethane inner sheath, where the sheath is removable by manipulation of the sheath flange seal that is accessible on an exterior of the introducer hub 908. In operation, the sheath flange 910 and 912 provides sealability against the device. This may allow for application of a biomarker element such as that shown in US Provisional Patent Application No. 62/375,421 filed on Aug. 15, 2016, the contents of which are incorporated herein. The introducer is shown in a "shortened" version in the drawings, but may be any appropriately configured length.

The disclosed assembly therefore allows quick and easy detection of biological contamination of a medical device on demand, i.e., such as during surgery. Accordingly, the disclosed assembly decreases the potential for using contaminated medical devices during medical procedures. Additionally, similar systems could be employed within any medical device, such as a syringe or other tools or working devices.

Some embodiments of the present invention may be utilized in applications other than those described herein. In some embodiments, the present invention may be used in other interior body regions or types of tissue. For example, certain embodiments of a medical device introduction system 10 of the present invention can be adapted for use in procedures related to the spinal column, for example, in the epidural space. In a particular embodiment, for example, the medical device introduction system according to the present invention may be utilized in an upright ventral epiduroscopic laser discectomy, in which the procedure is performed with the patient in an upright, symptomatic position such that diagnosis and treatment can be performed interactively with axial loading pressure on the affected intervertebral disc.

Features of a medical device introduction system and methods of the present invention may be accomplished singularly, or in combination, in one or more of the embodiments of the present invention. Although particular embodiments have been described, it should be recognized that these embodiments are merely illustrative of the principles of the present invention. Those of ordinary skill in the art will appreciate that a medical device introduction system 10 and method of the present invention may be constructed and implemented in other ways and embodiments. For example, in all cases, any of the features that are disclosed herein can be combined with any of the other features that are disclosed (even if those two or more distinct features appear in different sections of the above written, description). Accordingly, the description herein should not be read as limiting the present invention, as other embodiments also fall within the scope of the present invention.

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